Treatment of tibial shaft fractures in sheep using interlocking nails, Schanz screws and type I external fixators

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Abstract

This paper presents the results of a study of the treatment of transverse tibial shaft fractures in six sheep with the use of interlocking nails and type I external fixators. During surgery, tibial osteotomy was performed to induce an experimental fracture which was stabilized using a type I external fixator. Osteosynthesis was monitored for nine weeks by performing clinical tests, observing the degree of lameness and subjecting the patients to weekly radiological examinations. After nine weeks, the animals were euthanized, and samples of bone callus were sampled for histopathological analyses. Weight bearing on the fractured limb began on day 2 to 4 after treatment. Limb function was fully restored around five weeks after surgery. Radiograms taken during the observation period revealed gradual hyperplasia and progressing mineralization of bone callus at different stages of healing. The histopathological picture of the bone callus was characteristic of the phase of bone turnover and remodeling.

Key words: interlocking nail, bone, fracture, sheep

Introduction

Interlocking nail osteosynthesis is the leading method in the treatment of tibial fractures in humans (Krettek 1997, Folwarczny 2001). This technique is increasingly used in veterinary medicine, but new solutions are required to account for the differences in handling animal subjects. New generations of veterinary interlocking nails are developed to support such applications (Patii 2008, Piórek 2012). One of the latest solutions features a hybrid fixator which combines an interlocking nail with an external fixator system. This construct has been subjected to a series of in vitro biomechanical tests (Bemarde 2001, Radke 2006, Goett 2007), but in vivo studies are scarce (Moses 2002). The aim of this study was to evaluate the effectiveness of transverse tibial shaft fracture treatment in sheep with the use of interlocking nails and Schanz screws incorporated into a type I external fixator.

Materials and Methods

Experimental animals

The experiment was performed on six female hybrid Merino sheep, aged around 1.5 years, with body weight of 40 kg (+/- 5 kg). The animals were classified for the study based on radiograms of the left tibial
bone in medial and lateral projection. The length of the tibial bone and the width of the medullary cavity at the narrowest section were determined. The animals were kept under identical conditions in specially designed stalls. They were handled in accordance with the provisions of the Animal Protection Act. The study was approved by the Local Ethics Committee at the Faculty of Veterinary Medicine, University of Warmia and Mazury in Olsztyn, under resolution No. 26/2008/N of 29 May 2008.

**Fixator**

Nails and other elements of the external fixator were manufactured according to the author’s design by the Mikromed steelmill in Dąbrowa Górnicza. The nails were made of surgical Steel alloy (316 L) in three sizes (160 mm length with 6 mm and 8 mm diameter, 170 mm length with 8 mm diameter). Interlocking nails were solid rods with a circular cross-section and blunt ends. Each rod featured four transverse openings with a diameter of 4 mm for inserting interlocking screws, with two openings in the proximal section and two in the distal section of the nail. The openings were separated by intervals of 20 mm, inclusive of both ends of the nail. The proximal end was provided with a groove and an internal, longitudinal thread for attaching a guide. A guide was attached to the nail to ensure that pins were correctly aligned with the nail’s transverse openings. The interlocking process involved Schanz screws (180 mm length with 2.7 mm diameter) which served as half-pins of the external fixator. A titanium rod with a length of 170 mm and an internal diameter of 6 mm was the frame for the external fixator.

**Preoperative preparation, anesthesia and postoperative care**

Approximately one hour prior to surgery, the animals were premedicated with the antibiotic amoxicillin trihydrate (Betamox, Scanvet) at 20 mg/kg BW IM and metamizole (Biovetalgin, Biowet) at 50 mg/kg BW IM for pain relief. Directly before surgery, the patients were premedicated with xylazine (Vetaxyl; Vet-Agro) at 0.01 mg/kg BW IM. General anesthesia was induced by an infusion of 10% ketamine (Vetketam; Vet-Agro) at 22 mg/kg BW IV, and its doses were fractionated subject to the observed effect.

Patients were postoperatively administered the analgesic drug metamizol (Biovetalgin, Biowet), at 50 mg/kg BW IM for 6 days, and the antibiotic amoxicillin (Betamox, Scanvet), at 20 mg/kg BW SC every 48 hours for one week. The site of the implant was dressed, wound dressings were changed weekly and rinsed with 1% aqueous solution of chlorhexidine gluconate.

**Surgical procedure**

A skin incision with a length of 2-3 cm was made on the medial side of the mid-tibial shaft to produce an experimental fracture in the tibia. The bone was dissected with an oscillating saw.

The tibial bone stabilization procedure was initiated by making a skin incision with a length of ~ 0.5 cm on the medial side of the patellar ligament above the tibial tuberosity. The access on the tibial plane was used to insert a retractor and open the tibial medullary canal. A trocar was used to restore patency of the medullary canal and remove bone marrow. An intramedullary nail was inserted into the proximal fragment of the fractured bone. The above procedure facilitated maximum bending of the knee joint. The nail was inserted from the proximal section towards the distal end of the bone. The previously attached guide was rotated in a semi-circular fashion to facilitate the insertion of the nail. The nail was introduced into the proximal section of the bone to reduce the fracture, and it was further inserted towards the distal end of the bone. At the next stage of the procedure, the nail was fitted into the medullary canal, and was locked relative to the main fragments of the tibia using Schanz screws. The screws were placed in a cannulated guide to ensure that they were correctly aligned with transverse openings without radiological control. Skin incisions were made at the place of contact with the cannulas, and implants were inserted with the use of an orthopedic drill. Interlocking nails were inserted, and the guide was removed. At the last stage of the procedure, skin wounds were sutured using non-absorbable monofilament material (Monosof 2-0). Implants protruding above the skin were connected with the frame of the external fixator. The fixator was assembled, and screws were cut to length.

**Monitoring osteosynthesis**

Osteosynthesis was monitored by radiological examinations performed weekly, beginning on the day of surgery and ending after nine weeks. Radiograms were obtained using an SP-HF-4 device with the following settings: intensity of 4 mAs, tube voltage – 75 kV, distance from X-ray cassette – 100 cm, in two projections: side (medial – lateral) and sagittal (anterior – posterior). Bone union was evaluated on a four-point grading scale (Edwards 2004).
Table 1. Surgery time, clinical observations and evaluation of bone union.

<table>
<thead>
<tr>
<th>Sheep</th>
<th>Surgery time in minutes</th>
<th>Clinical observations</th>
<th>Bone union after 9 weeks of treatment</th>
</tr>
</thead>
<tbody>
<tr>
<td>1.</td>
<td>42</td>
<td>discharge in the area of implant in the distal fragment of the bone, loosening of implants in the distal fragment of the bone</td>
<td>++++</td>
</tr>
<tr>
<td>2.</td>
<td>38</td>
<td>loosening of the second implant</td>
<td>++++</td>
</tr>
<tr>
<td>3.</td>
<td>32</td>
<td>satisfactory implant anchoring</td>
<td>++++</td>
</tr>
<tr>
<td>4.</td>
<td>39</td>
<td>discharge in the area of implant in the distal fragment of the bone, loosening of implants</td>
<td>++++</td>
</tr>
<tr>
<td>5.</td>
<td>30</td>
<td>satisfactory implant anchoring</td>
<td>++++</td>
</tr>
<tr>
<td>6.</td>
<td>36</td>
<td>loosening of implant in the distal fragment of the bone</td>
<td>++++</td>
</tr>
</tbody>
</table>

Evaluation of bone union (Edwards 2004):
+ – weak
++ – fair
+++ – satisfactory
++++ – excellent

Table 2. Lameness assessment.

<table>
<thead>
<tr>
<th>Lameness</th>
<th>1st degree</th>
<th>2nd degree</th>
<th>3rd degree</th>
</tr>
</thead>
<tbody>
<tr>
<td>Sheep I</td>
<td>2 days</td>
<td>3 weeks</td>
<td>5 weeks</td>
</tr>
<tr>
<td>Sheep II</td>
<td>2 days</td>
<td>3 weeks</td>
<td>5 weeks</td>
</tr>
<tr>
<td>Sheep III</td>
<td>4 days</td>
<td>4 weeks</td>
<td>5 weeks</td>
</tr>
<tr>
<td>Sheep IV</td>
<td>4 days</td>
<td>3 weeks</td>
<td>5.5 weeks</td>
</tr>
<tr>
<td>Sheep V</td>
<td>3 days</td>
<td>3 weeks</td>
<td>5 weeks</td>
</tr>
<tr>
<td>Sheep VI</td>
<td>2 days</td>
<td>3 weeks</td>
<td>5 weeks</td>
</tr>
</tbody>
</table>

Patients were subjected to clinical examinations to determine the degree of lameness and full restoration of limb function. Lameness was evaluated based on the scale proposed by Braden and Brinker (Braden and Brinker 1973). The mobility of the stifle joint and the tarsal joint in the treated limb was monitored by comparison with the opposite leg (Durall 2004).

When bone union was achieved, the animals were euthanized using an overdose of intravenous pentobarbital. The fixator was disassembled, and the treated tibia was removed from the limb. The fracture site was subjected to a mechanical evaluation by attempting to manually bend and break the bone. Sections of the bone callus were stored in 10% neutralized formalin solution for further analysis.

Bone callus samples were decalcified in 100 g sodium citrate solution (C6H5O7Na3 x 2H2O), 250 g formic acid solution (CH2O2) and 250 g distilled water over a period of one month. Sections of calcified bone samples were obtained with a circular saw, and were decalcified for a further two weeks. The decalcifying agent was replaced three times during this period. Decalcified sections were embedded in paraffin in an autotechnicon (Microm STP 120 tissue processor, International GmbH) for 24 hours. The resulting paraffin blocks were cut in a sliding microtome (LEICA 2000R) into sections with a thickness of 3-5 μm. The sections were stained with hematoxylin and eosin, and subjected to histopathological analyses.

Results

The average time of surgical treatment was 36 minutes (30-42 min), counting from the moment of tibial osteotomy to incorporating screws into the external fixator (Table 1). Weight bearing on the fractured limb began on day 2 to 4 after treatment. Second degree lameness persisted for three weeks on average. Limb function was fully restored around five weeks after surgery (Table 2).

The results of clinical tests were within the norm. The mobility of stifle and tarsal joints in the treated limb did not deteriorate in comparison with the range of motion observed in the opposite leg. The presence of external elements of the fixator on the medial side
of the leg was well tolerated by the patients, and did not contribute to movement difficulties. Serous discharge was observed at the site of the implant in several patients (Table 1).

Radiograms taken during the observation period of nine weeks revealed gradual hyperplasia and progressive mineralization of bone callus at different stages of healing (Fig. 1). The images obtained one week after surgery showed a clear contour of the fracture groove. Two weeks after treatment, a light shadow indicative of small amounts of periosteal callus was observed in the fracture site in several patients. As a result of bone turnover and remodeling, the fracture groove began to disappear gradually after three weeks. Radiograms revealed clear periosteal shadows which bridged bone fragments and formed a cuff of callus around the fracture. In week 4, the fracture groove was visibly reduced, and the callus cuff was represented by a saturated shadow. Clear bridging between the fractured fragments was noted in several animals. The presence of bone union was observed starting in the fifth week after surgery. In weeks 6 and 7, the shadow cast by the bone callus was intensified, and was indicative of progressive bone mineralization. The fracture groove gradually faded away, and it disappeared completely towards the end of the observation period.

A mechanical evaluation which involved attempts to manually bend and break the bone revealed satisfactory strength of the bone callus. No signs of movement or springing of bone fragments were noted.

A histopathological examination of bone callus sections (Table 3) revealed compact bone tissue with normal trabeculae and intertrabecular substance. Spongy bone tissue had a regular structure, and comprised relatively thick trabecula and well-preserved bone marrow. In other layers of the tissue, trabecula were variously shaped and surrounded by numerous osteoblasts and bone marrow cells. The trabecula showed characteristic signs of bone turnover (Fig. 2). Fibroplastic foci were observed, and some of them contained numerous giant cells. Very large quantities of loose connective tissue and thick collagen fibers with multi-directional arrangement were found in the area of the bone fractures. Intense osteoplasia and numerous osteoblasts were noted in the region of preserved, compact bone tissue. Bone resorption, remodeling and osteoblast proliferation were observed (Fig. 3).

**Discussion**

In this experiment, the average time of surgical fixation was 36 minutes. In a study carried out by Lu, the procedure of stabilizing a tibial fracture lasted
Fig. 2. Histological view of bone scar – lamellar bone.

Fig. 3. Histological view of bone scar – bone remodeling.
around 90 minutes with the use of interlocking nails, and around 45 minutes when steel rods were embedded in osseous cement (Braid system) (Lu 2009). By comparison, only 15 minutes were needed to assemble the Maczek external fixator (Jąłysiński 1999).

The time of surgical fixation is significantly correlated with the risk of infection. According to Cruse and Foord, when other risk factors are excluded, the risk of infection doubles with every additional hour of surgery (Cruse 1980). In a study by Brown, the percentage of postoperative infections in a group of animals subjected to surgical treatment lasting 90 minutes was twice as high in comparison with patients where the procedure was completed in 60 minutes (Brown 1997). Prolonged surgery time increases the probability of infection, and the drying of exposed tissue during the procedure impairs its resistance (Vasseur 1988).

Weight bearing on the treated limb began sooner than in a study carried out with the involvement of the Maczek external fixator, where it started four to eight days after surgery (Jąłysiński 1999), but later than in an experiment with the Braid fixation which supported functional weight bearing directly after surgical treatment (Lu 2009). In a study where tibial fractures in sheep were treated with the use of a type I external fixation, Klein observed that non-weight bearing lasted for two weeks after surgery, after which weight was gradually applied on the treated limb (Klein 2003).

In dogs which underwent femoral osteotomy and fracture fixation with the use of interlocking nails incorporated in an external fixator, functional weight bearing on the affected limb was not noted in the first week after surgery (Durall 2004). An experiment investigating the osteosynthesis of the canine humerus with the use of interlocking nails provided similar results to those noted in our study. In the cited experiment, limb function was restored within four days after treatment, and it was described as satisfactory or excellent by the authors (Moses 2002).

The use of a type I external fixator in the treatment of limb fractures in sheep resulted in full recovery of limb function after six weeks (Klein 2003). In a study where standard interlocking nails were applied to fix tibial fractures in sheep, full recovery did not take place within nine weeks after the surgery (Klein 2004, Kaspar 2005). In a study by Auger, full restoration of limb function was noted after 7.5 weeks in dogs that had undergone tibial osteotomy and fracture fixation with the use of a type II external fixator (Auger 2002). In sheep fractures fixed with the Braid system or interlocking nails, recovery times ranged from eight to 12 weeks, but animals treated with the application of the Braid system were more likely to apply weight on the affected limb than the patients in which osteosynthesis was achieved with interlocking nails (Lu 2009).

According to Lu, early weight bearing after surgery involving the Braid fixation system reduces micro-motions at the fracture site (Lu et al. 2009). Micro-motions are caused by instability which is difficult to eliminate in fixation systems that rely on standard interlocking nails (von Pfeil et al. 2005, Dejardin et al. 2006). The work of Kaspar seems to corroborate the above findings (Kaspar et al. 2005).

In our study, functional weight bearing on the treated limb on the second day after surgery can be attributed to greater stability at the fracture site which was achieved by incorporating an interlocking nail with an external fixator. Our findings and the results reported by Klein seem to suggest that the use of a type I external fixator without interlocking nails is unlikely to eliminate micro-motions.

Early restoration of limb function has a positive effect on the further course of treatment. Functional weight bearing on the affected limb speeds up osteosynthesis and increases the strength of the bone callus (Sarmiento 1977, O'Sullivan 1994). According to Klein, the absence of functional weight bearing on the treated limb could produce long-term adverse consequences by delaying bone union (Klein 2004). Full weight bearing with insufficient fracture stabilization could, however, delay osteosynthesis (Augat 1997).

In the present experiment, bone union was observed in X-ray images obtained already in the fifth week of treatment. Radiograms taken in week 9 showed clear bridging between the fractured bone fragments in all sheep. In a study by Kaspar, osteosynthesis was noted after nine weeks of treatment involving interlocking nails and a modified system of screws. X-ray images obtained in the medial and lateral projection revealed the bridging of bone fragments at least in the cortical tissue in all patients. In the same experiment, in fractures treated with interlocking nails and standard screws which allowed for greater mobility of bone fragments, bridging was noted only in selected patients (Kaspar 2005). In the work of Lu, radiological examinations of fractures fixed with interlocking nails as well as the Braid system revealed bone union only in the 12th week of treatment (Lu 2009).

Examinations of bone fragment mobility supply valuable information about the quality of the callus formed. An absence of mobility testifies to the mechanical strength of the bone callus. Springiness of the fracture resulting from the flexibility of undeveloped callus is characteristic of early osteosynthesis, and indicates that bone turnover has not been completed.
(Białoszewski 2000). A mechanical evaluation which involved bending of the bone at the fracture site indicated satisfactory strength of the callus.

Histopathological evaluations of bone callus sections provide a detailed insight into osteosynthesis (Brighton 1991). The results of these analyses revealed correct bone union. The features of bone callus formed over the experimental period of nine weeks were characteristic of the stages of bone turnover and remodeling.

In this phase, the newly formed dense fibrous tissue is remodeled, and the remaining fragments of dead bone tissue are removed. This stage is characterized by intensified activity of osteoclasts which, together with osteoblasts, are responsible for bone turnover. The fracture site also features lamellar layers of compact bone tissue which reinforces the entire structure. Osteoclast activity is determined by the number of, and the distance from, osteoblasts. The highest levels of activity are noted in the region of the medullary cavity. Osteoclasts create resorption bays which are directly filled by bone marrow cells. This stage may continue for months or even years, and it ends with the achievement of complete bone union. Compact bone is transformed into lamellar bone, the medullary cavity and osteonic canals are restored together with normal length and shape of the bone (Niedźwiedzki 2007).

In a study of tibial fractures in sheep stabilized with a type I external fixator, histopathological analyses of the callus revealed complete bone union after nine weeks of treatment (Klein 2003, Klein 2004). The fracture groove was completely filled with mineralized bone tissue which bridged the fractured fragments (Klein 2004). In an experiment where tibial fractures in sheep were stabilized with interlocking nails, osteosynthesis was not achieved after nine weeks of therapy. The fracture site comprised mostly fibrous connective tissue, and the fractured fragments were completely bridged only on the lateral side of the bone. As demonstrated by biomechanical tests, stabilization techniques involving interlocking nails were less likely to counteract torsional forces than osteosynthesis methods involving external fixators (Klein 2004). Similar findings were reported by Kaspar who compared the treatment of bone fractures with the use of interlocking nails and standard screws vs. a modified system of screws that ensured a greater degree of rigidity between bone fragments (Kaspar 2005). In the above study, the callus formed after nine weeks of stabilization with a standard interlocking nail, was characterized by a larger cuff of connective tissue in comparison with fractures stabilized by a new interlocking system where the cuff was smaller and the callus comprised mostly mineralized compact bone tissue to indicate complete bone union. In a study comparing callus formations after six weeks of treatment with the involvement of various osteosynthesis techniques, Claes (1999) observed that the formation of internal callus is less intense in methods involving interlocking nails than techniques which rely on external fixators or bridging plates. Similarly to our study, the insertion of interlocking nails did not require openings in the medullary cavity; nevertheless, their presence disrupted blood supply to the inner bone. Ali osteosynthesis methods, excluding compression techniques, create flexible connections. In this type of stabilization, micro-motion is allowed between bone fragments, and this can both stimulate and inhibit bone union (Niedźwiedzki 2007). Fractured bone fragments become dislocated when transverse force is applied to the fracture line (Sumner-Smith 2002). When the force ceases to act, bone fragments return to their original position owing to the flexible structure of the applied fixator. The same spring-back effect can be generated by interlocking nails (Dueland 1996). In this process, the formation of external callus (Sumner-Smith 2002) is accompanied by the resorption of terminal bone fragments. The groove formed in the bone undergoing resorption is filled with new bone tissue. The formation of external callus begins along the outer edges of the bone, and chondroblasts appear between the fractured fragments. When a flexible connection is formed between those fragments, the callus is transformed into mineralized bone tissue. This process involves endochondral ossification between the periosteum and the endosteum and endochondral ossification between bone fragments; it initiates the remodeling phase in which woven bone is replaced by lamellar bone.

This study set out to evaluate the effectiveness of nail locking with the use of Schanz screws incorporated into an external fixator. The investigated construct proved to be an effective locking method which is useful in the treatment of fractures with the use of an external fixator. In some animals, small quantities of serous discharge were noted at the site of implant anchoring. Serous discharge is frequently noted when external fixators are used for osteosynthesis, and it results from interactions between the bone and the implant (Hyldahl 1991, Adamik 2010).

According to other authors, the main weaknesses of the investigated construct include poor anchoring in the cortical bone (Anderson 1993) due to negative threading of the nail, potentially higher risk of implant damage at the point when the threaded section of the nail passes into the unthreaded section, the risk of excessive implant depth which could irritate soft tissues and puncture the skin on the opposite side of the limb, and the need to cut the nails to length after fixator assembly.
Conclusion

The osteosynthesis technique which relies on an interlocking nail integrated with a type I external fixator is highly effective in the treatment of tibial shaft fractures in sheep, and supports quick restoration of limb function in the postoperative period. The use of a type I external stabilizer does not cause movement difficulty. The analyzed fixator is characterized by structural simplicity and ease of assembly. Schanz screws effectively block intramedullary nails and facilitate their incorporation with an external fixator.

References


