Influence of process parameters on content uniformity of a low dose active pharmaceutical ingredient in a tablet formulation according to GMP

The article describes the development and production of tablets using direct compression of powder mixtures. The aim was to describe the impact of filler particle size and the time of lubricant addition during mixing on content uniformity according to the Good Manufacturing Practice (GMP) process validation requirements. Processes are regulated by complex directives, forcing the producers to validate, using sophisticated methods, the content uniformity of intermediates as well as final products. Cutting down of production time and material, shortening of analyses, and fast and reliable statistic evaluation of results can reduce the final price without affecting product quality. The manufacturing process of directly compressed tablets containing the low dose active pharmaceutical ingredient (API) warfarin, with content uniformity passing validation criteria, is used as a model example. Statistic methods have proved that the manufacturing process is reproducible. Methods suitable for elucidation of various properties of the final blend, e.g., measurement of electrostatic charge by Faraday pail and evaluation of mutual influences of researched variables by partial least square (PLS) regression, were used. Using these methods, it was proved that the filler with higher particle size increased the content uniformity of both blends and the ensuing tablets. Addition of the lubricant, magnesium stearate, during the blending process improved the content uniformity of blends containing the filler with larger particles. This seems to be caused by reduced sampling error due to the suppression of electrostatic charge.

Keywords: content uniformity, warfarin, validation, narrow therapeutic index, Faraday pail, PLS regression

Development of dosage forms demands pharmacological and technological aspects, including suitably chosen statistic provability, to be taken into account from the very beginning. In narrow therapeutic index drugs, content uniformity is a critical parameter.

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Strict Good Manufacturing Practice (GMP) requirements concerning process validation of content uniformity to be met when transferring the production to the industrial scale should be followed as early as during laboratory development.

Pharmacological aspects of tablet blend content uniformity

Warfarin is used either as sodium salt or sodium salt isopropanol clathrate. Developed initially as rat poison, warfarin is still used as a first-line drug for thrombosis prevention in the USA, where tablets containing warfarin sodium salt have been marketed as Coumadine by DuPont Pharma since the 1950s. Patent protection expired by 1962; however, the narrow therapeutic index of warfarin prevented the production of generic substitutes. In 1980, switch to generic warfarin in the Boston City Hospital led to increased risk of mortality and health complications including acute bleeding (1). Wittkowsky suggests that extensive content uniformity limits may cause such complications. For example, a generic warfarin tablet labeled as containing 10 mg of drug might contain 8.50–11.50 mg according to EP 2.9.6 specification (85.0–115.0 %). The impact of this overlap is significant considering that when warfarin dosage is adjusted in response to alterations in therapy intensity, the dosage is typically increased or decreased by only 5–15 % of the daily dose. The original producer DuPont Pharma used the internal limit for content uniformity of 92.5–107.5 % with relative standard deviation (RSD) no more than 3 %, while the generic producer met the United States Pharmacopoeia (USP) limits of 85–115 % with RSD no more than 6 % (2). On the other hand, Jaffer and Bragg argued that the generic product contained amorphous warfarin, whereas the original product contained the salt in crystalline form. Amorphous warfarin could not be used in warfarin tablets in the USA any more (3). Until 1996, DuPont remained the sole producer of warfarin tablets in the USA. In September 1997, Food and Drug Administration (FDA) approved generic warfarin containing warfarin sodium salt clathrate, marketed by Barr Pharmaceuticals (now Teva). DuPont tried to stop the oncoming generic product and in 1996 asked the FDA to establish stricter limits in bioequivalence testing and to adopt its internal content uniformity limit as the USP standard. FDA declined both suggestions (4). Studies by Halkin (2003) (5) and Swenson (2005) (6) proved that the existing bioequivalence testing of generic substitutes was sufficient. Nevertheless, two important generic producers of warfarin tablets – Taro Pharmaceuticals and Apotex – introduced stricter internal limits for both bioequivalence and content uniformity, i.e., AUC and \( c_{\text{max}} \) within 0.8–1.25 with a confidence level 0.95 instead of 0.90, content uniformity within 92.5–107.5 % of the average and RSD not more than 3 % (7). In 2006, Barr Pharmaceuticals acquired the Croatian pharmaceutical producer Pliva Zagreb, together with its patent for warfarin tablets marketed in the USA. Content uniformity of these tablets was high, the content in all strengths ranged within 97–103 % of the average and RSD was not more than 2 %. The patent granted to the Croatian producer Pliva described warfarin tablets with possibly the highest content uniformity achieved so far (8). The procedure was based on the carrier impregnated with aqueous solution of warfarin sodium salt clathrate. Regardless of being crystalline or amorphous, the structure of warfarin used did not change after drying and further processing (9). It is clear that content uniformity remains an important issue when formulating solid dosage forms of drugs with a narrow therapeutic index. Similarly, Benet claims that complications during the treatment with narrow therapeutic index drugs API are mainly caused by inter-individual variability in drug quality (10).
Current GMP legislation concerning content uniformity

Regardless of how strict are the corporate internal limits for content uniformity, the quality of the product has to be tested in regular production according to the GMP. In fact, current legislation was inspired by Barr Laboratories, because in early 1990s FDA investigation in this company detected problems in content uniformity testing of solid dosage forms (11). In 1993, this resulted in an arbitrary court decision, ordering content uniformity testing of blends irrespective of validation process adequacy (12). Before that time, USP required content uniformity of 10 samples to fall within 85–115 % of the average and RSD not more than 6 %. This was narrowed to 90–110 % and RSD not more than 5 %. Sample mass should not exceed more than three times that of the final dosage form (12). These limits were listed in the FDA guidance (13). The decision was criticized, since there was no suitable sampling method that would eliminate sampling error. Parenteral Drug Association (PDA) reacted by issuing its Technical Report No. 25, suggesting a »holistic approach« to general analysis of the product. Under defined conditions, the error of failed content uniformity of the blend could be reconstructed from the error of passed content uniformity of the final product. However, the average content of the blend and the final product have to be statistically similar. More samples are required, both from one sampling place and from several sampling places (sample stratification). The error of blend content uniformity is equal to the sum of errors within one sampling place and product error within several sampling places (12). Following the discussion between the Product Quality Research Institute (PQRI), PDA and FDA, the latter issued a draft of new guidance (14), including a commentary (15), containing a more extensive description of the original limits based on stratified sampling. The FDA guidance documents were issued as the final guidance for industry and represent FDA’s current thinking on the topics covered. However, FDA’s guidance documents are not compulsory for either industry or the FDA. FDA accepts alternative approaches to those described in guidance documents, as long as the chosen approach is in accord with the applicable statute or regulation. On the other hand, USP monographs, harmonized with European Pharmacopoeia (EP) monographs, are obligatory.

Content uniformity validation

In the course of validation, the product has to meet defined requirements and specifications at a statistically significant confidence level. Validation covers also the stage of development, i.e., selection of excipients, procedure, and process parameters, including manufacturing process control, intermediates, final product and sampling. Content uniformity is a key parameter (16). Statistic methods offer several sophisticated models to evaluate the significance of the process (e.g., ANOVA). Nevertheless, experience suggests that complex equations demand professional statisticians. There are several simpler models where values are checked against tabulated data or are calculated easily. Use of capability indices $K$, $Cp$ and $Cpk$ enables the personnel to assess the correctness and precision of the process based on simple parameters demanded by the pharmacopoeia: average, maximum, minimum, and standard deviation (17). $Cpk$ index is defined as the lower value of upper and lower indices.

$$
\overline{Cpk} = \min \left[ \frac{USL - x_i - LSL}{3s}, \frac{x_i - LSL}{3s} \right]
$$

$i(1)$

$USL$ – upper specified limit, $LSL$ – lower specified limit, $x_i$ – average, $s$ – standard deviation.
If the result is not less than 1.0, at least 99.73 % of batches produced by this process will pass the applied acceptability criterion. This limit is suitable for content uniformity validation. Other simple methods include standard deviation predilection interval (SDPI) or Bergum division adapted to suit the USP monograph «uniformity of dosage units» <905> and its harmonized European counterpart (2.9.40). Bergum criterion is based on tabulated RSD value which guarantees, with 90.0 % certainty, that at least 95.0 % of samples tested for content uniformity will pass the <905> USP test (18).

**Impact of composition and procedure on content uniformity**

To reach uniform content of a low dose drug in the final dosage form while keeping the production costs low, a suitable tablet composition and procedure have to be chosen. The easiest method for tablet production is direct compression, where all constituents are weighed and mixed in a single container. Turbula is a reliable and efficient 3D mixing device that can be used not only in the development but also in scale-up production (19). With this device, final content uniformity is influenced by the ratio of constituents and the active ingredient, electrostatic charge, particle density, shape and size. Significant procedural parameters include the mixing order of individual components, mixing time and speed, container shape and container load (20). The highest degree of content uniformity can be reached if the shape, size and density of mixed particles are as similar as possible; spherical shape is preferred. The ratio of active substance and excipients should be equal and there should not be any electrostatic charge (21). If the mixing time is too short, the blend is not mixed properly; on the other hand, if the mixing time is too long, «overmixing» can occur and the constituents will separate in dependence on their differing properties. The results are almost impossible to estimate in advance and the above mentioned recommendations cannot be fulfilled. Particle size, shape and density are usually dissimilar and electrostatic charge changes in the course of the manufacturing process (22). Applied composition is thus a compromise between general recommendations and real requirements.

**Experiment design and hypothesis**

The goal was to assess the impact of particle size distribution of the filler, in this case calcium hydrogen phosphate, on content uniformity of the blend in relation to the addition of magnesium stearate at various stages of the mixing process. The composition is based on previous experiments (23); the procedure of »common blend« was used where tablets of various strengths (1 to 10 mg) were compressed from the same blend by changing the tablet mass (approximately 50 to 500 mg). A single validated blend containing 2 % of warfarin sodium salt clathrate was used for the production of tablets of all strengths.

Content uniformity of the tableting blend had to meet EP (2.9.6) and FDA requirements and the results were evaluated using the Cpk index. Final product content uniformity had to meet USP (<905>) and EP (2.9.6, 2.9.40) requirements and the results were evaluated using the Cpk index and Bergum division. Tablets had to meet also internal DuPont requirements of 92.5–107.5 % of the labeled drug strength, and RSD not more than 3 %.

We planned to find out if demixing of the blend during the process could be caused by electrostatic charge forming in the blend during blending.
Partial least squares (PLS) regression was used to fully evaluate the impact of studied variables on content uniformity.

**EXPERIMENTAL**

**Tableting blend and tablets**

Blend composition and some of its physicochemical properties are listed in Table I. All constituents were sieved through a 250 µm sieve and mixed for 15 minutes (procedure A) or all constituents, without magnesium stearate, were mixed for 10 minutes, then magnesium stearate was added and another 5 minutes of mixing followed (procedure B). A Turbula homogenizer (T2C, Switzerland) was used, speed 40 rpm. Mass of one batch was 500.0 g. Four blends were prepared (2 compositions, 2 procedures). Flat tablets with a diameter of 7 mm, mass about 200 mg, and hardness about 70 N were produced using an eccentric press (Korsch EK0, Germany). Two batches were produced for every procedure/composition combination. An additional third batch was produced using the composition and procedure that showed the best results.

**Sampling and warfarin content measurement**

Tableting blend was placed in a cylindrical vessel of 25 cm diameter and was leveled to a height of about 2 cm by slight horizontal movement. The area was then divided evenly into 10 parts; out of each of these parts, a sample weighing approximately three times more than the tablet was taken with a small spoon. Samples were weighed with 0.1 mg

<table>
<thead>
<tr>
<th>Component</th>
<th>Producer</th>
<th>Density [kg m⁻³]</th>
<th>Particle size (µm)</th>
<th>Content (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td></td>
<td></td>
<td>D₁₀</td>
<td>D₅₀</td>
</tr>
<tr>
<td>Warfarin</td>
<td>Pliva (Croatia)</td>
<td>1312.8</td>
<td>2.5</td>
<td>10.3</td>
</tr>
<tr>
<td>Di-cafos 92-12</td>
<td>Budenheim KG (Germany)</td>
<td>2881.5</td>
<td>36.1</td>
<td>61.1</td>
</tr>
<tr>
<td>Di-cafos 92-14</td>
<td>Budenheim KG (Germany)</td>
<td>2937.9</td>
<td>2.4</td>
<td>152.3</td>
</tr>
<tr>
<td>Avicel pH 101</td>
<td>FMC BioPolymer (USA)</td>
<td>1572.4</td>
<td>14.7</td>
<td>46.3</td>
</tr>
<tr>
<td>Ac-Di-Sol</td>
<td>FMC BioPolymer (USA)</td>
<td>1611.5</td>
<td>12.2</td>
<td>33.1</td>
</tr>
<tr>
<td>Magnesium stearate</td>
<td>Peter Greven (Germany)</td>
<td>1085.9</td>
<td>2.6</td>
<td>10.2</td>
</tr>
</tbody>
</table>

*Dᵩ = x % of measured particles smaller than this size (µm); Di-cafos – calcium hydrogen phosphate; Avicel PH 101 – microcrystalline cellulose; Ac-Di-Sol – sodium croscarmellose
precision, transferred quantitatively to 100 mL flasks and water was added. Tablets were sampled during the tableting process so that 10 tablets from each batch were taken at regular intervals. Tablets were weighed, put into flasks and let to dissolve for 12 hours in a mixture of water and methanol (9:1, V/V). From both the blend and tablet samples, insoluble excipients were removed by a centrifuge for 10 minutes and at 15000 rpm (SIGMA Laborzentrifugen 2K15, Germany) and samples were analyzed by HPLC. Warfarin content was measured using the calibration curve.

We used a high performance liquid chromatograph YL 9100 (Young Lin Instrument, Korea) with a quaternary pump, automatic sampler and diode array detector. The separation column was BDS HYPERSIL C18 (150 × 4.6 mm; particle size 5 µm). Analysis conditions: mobile phase methanol (64 %) and formic acid (0.04 mol L⁻¹, 36 %), flow rate 1.4 mL min⁻¹, column temperature 25 °C, analysis wavelength 280 nm, sample size 20 µL, analysis time 7 minutes.

Charge measurement

The charge was measured in individually prepared model mixtures. Their composition was designed so as to find out the impact of the carrier particle size along with addition of magnesium stearate on the final electrostatic charge. For the preparation of model mixtures, an identical procedure was applied as in the preparation of tableting blends. Fillers alone (Di-cafos 92–12, Di-cafos 92–14), their mixtures with warfarin and their mixtures with warfarin and magnesium stearate were used as model samples. Fillers alone and their mixtures with warfarin were mixed for 10 minutes; when magnesium stearate was added, additional 5 minutes of mixing followed.

Electrostatic charge was measured using a Faraday pail of standard construction, consisting of the outer insulating and inner measurement pail (24). The sample transfers its charge to the inner pail and voltage change between the inner pail and the ground is measured. Complete volume of the model mixture weighing 80 g (measurement repeated three times) was poured directly from the glass homogenization vessel to the inner cup of 250 mL volume and the measured charge was calculated to correspond to 1 g of sample.

Statistical data analysis

Results of individual samples (n = 10) from each batch were recalculated according to the theoretical warfarin content in the blend. Average content, standard deviation and relative standard deviation were calculated for every batch. Statistical evaluation of variance for both compositions and both procedures was performed using the F-test of equality of variances (QC.Expert 3.2., TriloByte). To evaluate the impact of procedure variables (filler particle size, time of magnesium stearate addition) and their interaction with response variables (RSD, Cpk of EP 2.9.6 criteria, Cpk of FDA criteria), PLS regression was used, including the Martens uncertainty test (25). Prior to modeling, response variables were automatically adjusted by autoscaling, which uses mean-centering followed by the dividing of each variable by its standard deviation. Design evaluation was performed with Unscrambler X (v. 10.3, Camo software).
Blends and tablets that were manufactured differed in the filler particle size distribution and in the time when lubricant was added in the mixing process. Mixing time of 15 minutes was chosen on the basis of previous experiments with similar composition where the impact of mixing time, different types of fillers and different particle size distribution of warfarin on content uniformity were tested (23, 26). Magnesium stearate was added either at the beginning of mixing or after 10 minutes. The results show that the chosen variables affected warfarin content uniformity of the tableting blend (Table II). If the filler with larger particle size \(D_{50} = 152 \, \mu\text{m}\) was used, content uniformity was better than in the case of smaller particle size \(D_{50} = 61 \, \mu\text{m}\). Results for both procedures and compositions were compared by the F-test of equality of variances \((p \leq 0.05)\). Statistical evaluation proved a significantly smaller variance of the measured content in blends prepared with fillers of larger particle size (Di-cafos 92-14; \(D_{50} = 152 \, \mu\text{m}\)). This applies to both procedures, which differed in the time when lubricant was added. The influence of the procedure used on the final variance of warfarin content was also evaluated by the \(F\)-test of equality of variances. The test did not reveal any statistically significant difference in the variance of warfarin content in blends prepared by procedures A and B (Table II). This applied to blends with both larger and smaller filler particle size. This points to the conclusion that when using either procedure, the critical parameter for reaching the required content uniformity is the filler particle size distribution.

The time when lubricant was added did not have a statistically significant impact on the measured variance of warfarin content in manufactured blends. Physical bonds between magnesium stearate and lubricated particles were weaker than in the absence of lubricant (27). Magnesium stearate may influence the intensity of physical bonds, \textit{i.e.},

\[\text{Table II. Average content and content uniformity parameters of blends}\]

<table>
<thead>
<tr>
<th>Batch(^a)</th>
<th>(x^b) (%)</th>
<th>RSD</th>
<th>EP(^c) (2.9.6)</th>
<th>FDA(^c)</th>
<th>Cpk(^d) (\text{(FDA)})</th>
<th>Cpk(^d) (\text{(FDA)})</th>
</tr>
</thead>
<tbody>
<tr>
<td>1_A_D61</td>
<td>103.0</td>
<td>6.24</td>
<td>+</td>
<td>–</td>
<td>0.62</td>
<td>0.36</td>
</tr>
<tr>
<td>2_A_D61</td>
<td>100.3</td>
<td>5.53</td>
<td>+</td>
<td>–</td>
<td>0.88</td>
<td>0.58</td>
</tr>
<tr>
<td>1_A_D152</td>
<td>98.0</td>
<td>3.06</td>
<td>+</td>
<td>+</td>
<td>1.45</td>
<td>0.89</td>
</tr>
<tr>
<td>2_A_D152</td>
<td>100.1</td>
<td>2.58</td>
<td>+</td>
<td>+</td>
<td>1.92</td>
<td>1.27</td>
</tr>
<tr>
<td>1_B_D61</td>
<td>103.3</td>
<td>3.41</td>
<td>+</td>
<td>+</td>
<td>1.07</td>
<td>0.62</td>
</tr>
<tr>
<td>2_B_D61</td>
<td>102.3</td>
<td>7.18</td>
<td>–</td>
<td>–</td>
<td>0.56</td>
<td>0.34</td>
</tr>
<tr>
<td>1_B_D152</td>
<td>100.5</td>
<td>1.37</td>
<td>+</td>
<td>+</td>
<td>3.50</td>
<td>2.29</td>
</tr>
<tr>
<td>2_B_D152</td>
<td>99.3</td>
<td>1.76</td>
<td>+</td>
<td>+</td>
<td>2.72</td>
<td>1.77</td>
</tr>
<tr>
<td>3_B_D152</td>
<td>102.2</td>
<td>2.06</td>
<td>+</td>
<td>+</td>
<td>2.04</td>
<td>1.24</td>
</tr>
</tbody>
</table>

\(^a\)Batch label: batch number_procedure_filler particle size \(D_{50}\) (50 % of particles smaller either than 61 or 152 \(\mu\text{m}\));
\(^b\)average of 10 samples from a particular batch; \(^c\) (+) passed, (–) failed; \(^d\) Cpk values calculated according to Equation 1.
trostatic bonds and Van der Waals bonds, which can have an impact on content uniformity by decreasing the electrostatic charge of blended part.

Electrostatic charge was measured to try to explain the observed impact of filler particle size on content uniformity. The impact of added magnesium stearate on the magnitude of electrostatic charge was measured with the Faraday pail in model blends containing the active substance only (warfarin sodium salt clathrate) and filler (calcium hydrogen phosphate) of various particle sizes (Table III). The composition of these model mixtures was chosen so as to eliminate the impact of other excipients (Avicel and Ac-Di-Sol) on the final electrostatic charge.

Measurements showed that neither filler itself nor its blends with warfarin differed in charge in a statistically significant way. However, when magnesium stearate was added, statistically significant changes in electrostatic charge occurred. When the filler of larger particle size was used, the change in electrostatic charge was lower than in the filler of smaller particle size. When magnesium stearate was added, the value of electric charge changed its polarity. This influence of magnesium stearate was already described (27). These results may explain better uniformity of blends containing the filler of larger particle size because the electrostatic charge was reduced. Charge can have a negative impact on uniformity or increase the possibility of sampling error. Experience shows that if the blend has lower content uniformity than tablets and there is no further homogenization during compression, there has to be an error in blend sampling (12). As the difference in uniformity of individual blends was higher than in uniformity of tablets produced from them (see Table II and V), this was probably a sampling error (e.g., adhesion of blend components to the sampler surface caused by electrostatic charge). Particle size of mixed constituents has an impact on uniformity by itself (e.g., movement of particles) or in connection with some other commonly used excipients, e.g., magnesium stearate, which influences physical bonds between particles with respect to their size.

Although experimentation was run on a laboratory scale, tableting blends were evaluated according to validation criteria used in production transfer on a larger scale, corresponding to GMP requirements for validation. We used criteria from EP 2.9.6, which states

### Table III. Total electrostatic charges of model blends

<table>
<thead>
<tr>
<th>Componentsa</th>
<th>Electrostatic charge (nC g⁻¹)d</th>
</tr>
</thead>
<tbody>
<tr>
<td>D61a</td>
<td>0.042 ± 0.031</td>
</tr>
<tr>
<td>D61 + Wb</td>
<td>0.083 ± 0.014</td>
</tr>
<tr>
<td>Blend with D61c</td>
<td>−0.165 ± 0.041</td>
</tr>
<tr>
<td>D152e</td>
<td>0.042 ± 0.007</td>
</tr>
<tr>
<td>D152 + Wb</td>
<td>0.083 ± 0.019</td>
</tr>
<tr>
<td>Blend with D152c</td>
<td>−0.054 ± 0.007</td>
</tr>
</tbody>
</table>

a Di-cafos only (D61 or D152 according to particle size); b blend of Di-Cafos with warfarin (W); c tableting blend prepared by procedure B (i.e., magnesium stearate was added after 10 minutes of blending); d average of three measurements ± standard deviation.
that the content of active substance in each of 10 samples has to be within 85–115 % of average content as well as criteria from FDA guidance which states that each sample has to contain 90–110 % of average content and RSD has to be lower than 5 %. Cpk indices were calculated for both EP and FDA limits: for validation of solid dosage forms, Cpk must not be less than 1.0. Tableting blends prepared from the filler of larger particle size met all validation criteria, which is consistent with the above mentioned facts. The time when magnesium stearate was added to the blend was found to be significant; only batches where magnesium stearate was added in the course of mixing met the FDA requirement,
confirmed at the required statistical significance level \( Cpk \geq 1 \) (Table II). Although the current FDA guidance no longer considers the use of traditional three-batch validation appropriate, it does not prescribe the number of validation batches for a prospective validation protocol (28). A third batch based on this procedure and composition was prepared and expected to strengthen statistical data and help scale up the production. This third batch also met all validation criteria. PLS regression was used to fully describe the impact of studied technological variables (filler particle size, time of lubricant addition) on response variables (RSD, \( Cpk \) pursuant to EP 2.9.6 criteria, \( Cpk \) pursuant to FDA criteria) of prepared blends. One of the PLS model outputs is the PLS-ANOVA summary table, which shows \( p \)-values of the effects of respective procedural variables and their interactions with response variables. If the \( p \)-value of effect is not higher than 5 \%, the effect is considered to be significant. If the value ranges between 5 and 10 \%, the effect is marginally significant. Design evaluation by PLS regression is suitable because there is no limit to the number of experiments. Co-variance between response variables is taken into account, which enables a study of their mutual dependence. Graphic simplification of dependence between procedural and response variables is usually presented as a correlation loading plot, where significant correlations \( (R^2 > 0.5) \) are marked by Hotteling’s ellipse. An advantage is the possibility of using un-controlled response variables in the experiment and finding out if they have an impact on the quality of the model. On the other hand, it must be said that it is not possible to get real \( p \)-values but only their estimation (29, 30).

The developed PLS model describes quantitatively the dependence between the matrix of X procedural variables (filler particle size, time lubricant addition) and the matrix

![Correlation-loading plot](image_url)

**Fig. 1.** Correlation-loading plot showing relationships between the procedural variables and their interactions of X-matrix (boxes) and responses of Y-matrix (circles). Technological variables labeled in the form of the applied procedure (A or B), filler particle size (D61 or D152) and their interactions (A*D61; A*D152; B*D61; B*D152). Response variables labeled in the form of RSD, \( Cpk \) for EP 2.9.6 criteria and \( Cpk \) for FDA criteria.
of \( Y \) response variables (RSD, \( C_{pk} \) pursuant to EP 2.9.6 criteria, \( C_{pk} \) pursuant to FDA criteria). The resulting correlation loading plot (Fig. 1) describes, using the first two components, 63 and 87% of total variability of matrices \( X \) and \( Y \), respectively. The distribution of variables in the outer area of Hotelling's ellipse suggests a significant impact \( (p < 0.05) \) of particle size \( (D_{61}; D_{152}) \) on \( RSD \) value. It is possible to claim that the use of procedure B in combination with larger particles caused a significant decrease in \( RSD \) and a potentially significant increase \( (0.05 \leq p < 0.1) \) in both \( C_{pk} \) values. This is the reason why this combination of procedure B and larger filler particle size \( (B*D_{152}) \) can be considered more suitable for attaining good content uniformity than the combination of procedure A and smaller filler particle size \( (A*D_{61}) \). There is a potentially significant impact \( (0.05 \leq p < 0.1) \) on increased \( RSD \) and decreased \( C_{pk} \). Figure 1 shows a narrow correlation between both \( C_{pk} \) values, which is also clear from the minimum difference between \( p\)-values in Table I. These findings confirm the uniformity results according to validation criteria, when all criteria were met only by blends prepared by procedure B from the filler with larger particle size.

Blends were processed into tablets, in which warfarin content was measured, evaluated statistically and according to validation criteria similarly to the tableting blend (Table V). The results obtained from tablets originating from fillers of different particle size (procedure A or B) were compared by the \( F \)-test of equality of variances \( (p \leq 0.05) \). For procedure A, this statistical evaluation proved a significantly lower variance of the measured content of active substance in tablets when the filler of larger particle size was used. For procedure B, no statistically significant impact was found. As there was a statistically significant difference between tableting blends and tablets from the same batches, it seems probable that content uniformity was correct but there was a sampling error. This claim corresponds to the measured growth of overall electrostatic charge in blends prepared from the filler of smaller particle size (Table III). Electrostatic charge can have a negative impact on sampling, which was probably the main cause of poorer content uniformity of these blends. Similarly to the blend, there was no statistically significant difference in the measured contents in tablets \( (F\text{-test of equality of variances}) \) between procedures A and B, \textit{i.e.}, the time when lubricant was added to the blend. Tablets were evaluated according to validation criteria (Table V) common for the production of solid dosage forms. EP monographs 2.9.6 and 2.9.40, \( C_{pk} \) index for 2.9.6 monograph limits (85–115%) and Bergum division were used. Bergum division offers tabulated \( RSD \) values that ensure, on a 90% confidence level with 95% probability, that subsequently produced batches will pass EP monograph 2.9.40. Validation criteria were met only in tablets manufactured with the filler of larger particle size.

CONCLUSIONS

The paper describes the methods used in process validation of solid dosage form manufacture. A model dosage form, tablets with low API content, containing warfarin, was used to evaluate the impact of particle size distribution of the used filler and the time when lubricant was added on blend and tablet content uniformity. Content uniformity was evaluated according to validation and pharmacopoeial criteria. The results show that both evaluated variables (filler particle size and time of lubricant addition) had an impact on
content uniformity. The highest content uniformity of blend and tablets was found for the filler of particle size $D_{50} = 152$ µm combined with magnesium stearate added later in the blending process (technology B). Cpk index and Bergum division proved that this blend and tablets meet pharmacopeial criteria as well as FDA GMP scale-up content uniformity criteria at a statistically high level. Differences between blends and tablets manufactured from them ($D_{50} = 61$ µm, technology B) are probably caused by the blend sampling error. Electrostatic charge formed during the blending may play a major role in this error. Electrostatic charge measurements of model mixtures are in accord with the assumption that a higher electrostatic charge of the mixture may cause a blend sampling error (e.g., adherence of material to sampler surface). This experience should contribute to the future development of safe drugs containing a small amount of highly efficient APIs manufactured by direct compression.


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